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Microtensile dentin bond strength evaluation of different adhesive systems: *in vitro* study

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Microtensile dentin bond strength evaluation of different adhesive systems: *in vitro* study

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Abstract

Introduction: Modern restorative dentistry has been extensively influenced by the fast progress in dental adhesive technology. To assess the effectiveness of adhesive systems and to predict their clinical performance the resin-dentin bond strength tests has been widely used.

Purpose: The goal of this study was to compare the microtensile bond strength of five different adhesives systems at the dentin-composite interface and evaluate failure modes.

Materials and methods: Flat dentin surfaces were prepared in 25 non-carious human molars. Exposed dentin surfaces were wet-grounded with 240-, 400- and 600-grit silicon-carbide sandpaper to create bonding surfaces with a standardized smear layer. The teeth were randomly divided into 5 distinct groups according to the adhesive system tested: three self-etching adhesive systems, Xeno[®] V+ (Dentsply DeTrey, Konstanz, Germany); Xeno[®] III (Dentsply DeTrey, Konstanz, Germany) and Clearfil[™] SE Bond (Kuraray Medical Inc., Okayama, Japan), and two etch-and-rinse adhesive systems, OptiBond[™] FL (Kerr, Orange, CA, USA) and Prime&Bond[®] NT (Dentsply DeTrey, Konstanz, Germany) applied with respect to manufacturer's instructions. After adhesive procedures a 4-mm thick composite crown was built over the bonded surface. Following the storage in distilled water at 37 °C, the samples were vertically cross-sectioned until obtaining sticks with 1.37mm² of cross-sectional area which were tested in tension in a universal testing machine at 0.5 mm/min. Data were analyzed by one-away ANOVA and a Tukey HSD post-hoc test (p<0.05). The mode of failure was also analysed with optical microscopy. Additionally, dentin disks were obtained, treated with the different conditioners and primers and observed by scanning electron microscopy (SEM).

Results: The following microtensile bond strengths were registered (mean in MPa±SD): Group I – Xeno[®] V+ 3.70±5.01; Group II - Xeno[®] III 18.94±13.87; Group III – OptiBondTM FL 43.29±12.74; Group IV- Prime&Bond[®] NT 39.64±15.06 and Group V – ClearfilTM SE Bond 42.80±10.65. Etch-and-rinse (OptiBondTM FL; Prime & Bond[®] NT) and two-step self-etching (ClearfilTM SE Bond) adhesive systems attained significant higher microtensile bond strength, without statistically significant differences between them. Significant lower values were obtained for Xeno[®] V+ comparing to Xeno[®] III. Cohesive

composite failures were related with the higher bond strength values, whereas the adhesive failures were associated with the lowest bond strength values.

Conclusion: Among the materials evaluated, etch-and-rinse and two-step selfetching adhesive systems presented higher dentin bond strength than the one-step selfetching adhesive systems.

Keywords: microtensile; dentin bond strength; etch-and-rinse; self-etch; dentin adhesion

Introduction

Improvements in dental adhesive technology have extensively influenced modern restorative dentistry¹. Today's, operative dentistry should primary involve "minimally invasive" techniques^{1, 2} that promotes a more conservative cavity design, which basically relies on the effectiveness of current enamel-dentine adhesives¹.

Bonding to enamel has been demonstrated to be easy and durable while bonding to dentin is far more challenging³, due to the heterogeneity of structure and composition of dentin, its surface characteristics after bur cutting and chemical treatments^{1, 3-7} and relation with pulpal tissue by means of numerous fluid-filled tubules¹. Basically, current dentin adhesives employ two different means to achieve the goal of retention between restorative material and dentin⁸: by removing the smear layer with etch-and-rinse adhesives or modifying the smear layer with self-etch adhesives.

The adhesion to tooth substrate implies an exchange process in which some inorganic tooth material is removed and replaced by resin monomers^{2, 9} that, upon polymerization, become micromechanically interlocked in the created microporosities^{10, 11}, rather than on a primary chemical adhesion¹². However, this twofold bonding mechanism is believed to be advantageous in terms of restoration longevity^{13,14}.

Contemporary dental adhesive systems can be classified according to the application techniques as etch-and-rinse and self-etching adhesives systems¹⁵. In the first one, the acid-etching application completely removes the smear layer, followed by the application of primer and bond resin in one or two steps¹⁶. The etch-and-rinse technique is still the most effective and stable approach for enamel bonding². However, concerning dentin bonding, this technique can be considered to be difficult and less predictable¹. With the self-etching adhesive systems the clinician can simplify the clinical procedures and also reducing clinical time¹⁷, therefore to reduce technique sensitivity or risk of making errors during application and manipulation². Nevertheless, some potential problems are related with the use of some self-etching adhesives, like postoperative sensivity, incomplete marginal seal, premature bond degradation, biocompatibility, and compromised bonding to abnormal substrates¹⁸.

The self-etch technique does not require a separating etching step, it uses acidic monomers that simultaneously etch and prime the dental substrate¹. The self-etch adhesive systems can be classified according to the pH of the adhesive solutions in strong (pH<1), intermediately strong or moderate (pH between 1.0 and 2.0) and mild $(pH>2)^2$. The high acidity results in rather deep demineralization effects. So, the bonding mechanism of "strong" self-etching adhesives can be similar to the etch-and-rinse approach². However, low-pH self-etch adhesives reveals low bond strength values, especially at dentin² with a high number of pre-testing failures, especially when tested with a microtensile methodology².

The aim of this study was to compare the dentin microtensile bond strength of five adhesive systems.

The null hypothesis was that there were no significant differences between the five adhesives systems evaluated.

Materials and methods

Specimen preparation

Twenty-five non-carious human molars were collected and stored in distilled water within 10 weeks after extraction. The teeth were cleaned from debris and partially included in an acrylic resin block (Orthocryl[®], Dentaurum). The oclusal surfaces were cut perpendicularly to the long axis of the tooth (Accutom 5, Struers, Ballerup, Denmark), under water-cooling, thereby exposing a flat dentin surface without residual enamel. All oclusal surfaces were wet-ground with a sequence of 240-, 400- and 600-grit silicon-carbide sandpaper in circular motion for 60 seconds to obtain a uniform smear layer. The prepared oclusal surfaces were carefully observed using an optical microscope at a 40-fold magnification (M300, Leica, Switzerland) to confirm the absence of residual enamel or another defects in dentin surfaces.

Bonding and restorative procedures

The teeth were randomly divided in five groups, according the five adhesive systems tested: two and three-step etch-and-rinse adhesives and one and two-step self-etch adhesives (Table I).

Adhesive	Manufacturer	Chemical Composition	рН	Batch no.
Group I Xeno® V+ 1-step/ 1 bottle Self-etch Adhesive	Dentsply DeTrey, Konstanz, Germany	-Bifunctional acrylate -Acidic acrylate - Functionalized phosphoric acid ester -Water -Tertiary butanol -Initiator - Stabilizer	1.3 ¹⁹	1203000016
Group II Xeno® III 1-step/ 2 bottles Self-etch Adhesive	Dentsply DeTrey, Konstanz, Germany	Liquid A: -HEMA; purified water; ethanol; BHT; highly disperse silicone dioxide Liquid B: -Pyro-EMA; PEM-F; urethane dimethacrylate; BHT; camphorquinone; ethyl-4-dimethylaminobenzoate	1.4 ²	1302000019
Group III OptiBond [™] FL 3-step Etch-and-rinse adhesive	Kerr, Orange, CA, USA	Etchant: 37.5% phosphoric acid <u>Primer</u> : -HEMA;GPDM; PAMM; ethanol; water; photo initiator <u>Adhesive</u> : - TEGDMA; UDMA; GPDM; HEMA; bis-GMA; filler; photo initiator	1.8 ²	4677483

 Table I: Adhesive systems studied, manufacturers, chemical composition, pH values and batch numbers.

Group IV Prime&Bond® NT 2-step Etch-and-rinse adhesive	Dentsply DeTrey, Konstanz, Germany	-Di-and trimethacrylate resins -PENTA -Photoinitiators -Stabilizers -Acetone -Nanofillers	2.2 ²	1206000730
Group V Clearfil [™] SE Bond 2-step Self-etch Adhesive	Kuraray, Okayama, Japan	Primer: 10-MDP; HEMA; hydrophilic aliphatic dimethacrylate; dl-camphorquinone; N,N-Diethanol-p-toluidine; water Adhesive: Bis-GMA; 10-MDP; HEMA; hydrophobic aliphatic dimethacrylate; dl-camphorquinone; N,N-Diethanol-p-toluidine; colloidal silica	1.9 ²	041931

BHT: Butylated hydroxyl toluene; **Bis-GMA:** Bisphenol A diglyciyl methacrylated; **GPDM:** glycerol phosphate dimethacrylate; **HEMA:** 2-hydroxyethl methacrylate; **PAAM:** Phthalic acid monoethyl methacrylated; **PEM-F:** Mono fluoro phosphazene modified methacrylate; **PENTA:** Dipentaerythritol pentaacrylate phosphate; **PYRO-EMA:** Phosporic acid modified methacrylate; **MDP:** methacryloyloxydecyl; **TEGDMA:** triethylene glycol dimethacrylate; **UDMA:** Urethane dimethacrylate;

The bonding and light-curing procedures were carried out as recommended by each manufacturer (Table II).

Group/ Adhesive system	Application procedure
I - Xeno [®] V+	Apply actively adhesive for 20 sec; air-drying for 5 sec; light-curing for 10 sec.
II - Xeno [®] III	Mixing equal amount of Liquid A and B for 5 sec; apply actively for at least 20 sec; air-drying; light-curing for 10 sec
III - OptiBond [™] FL	Apply 37.5% phosphoric acid (Kerr Gel Etchant®) for 15 sec; rinse for 15 sec; gently air-dry; apply primer actively for 15 sec; gently air-dry for 5 sec; apply the adhesive for 15 sec air-dry for 3 sec; light-curing for 20 sec.
IV - Prime & Bond [®] NT	Apply 36% phosphoric acid for 15 sec; Spray and rinse with water for 15 sec; blot dry conditioned areas; apply adhesive and leave the surface wet for 20 sec; gently air-dry for at least 5 sec; Polymerize for 10 sec; apply a second layer of adhesive in similar way.
V - Clearfil [™] SE Bond	Apply primer for 20 sec; mild air stream; apply bond; gentle air stream; light- curing for 10 sec.

Table II: Adhesive application procedures (according manufacture recomentations).

Following the bonding procedures, the crowns of the cut teeth were reconstructed with three incremental layers (1.5 mm) of light-cured microhybrid composite resin Esthet.X[®] HD A2 (DentsplyDeTrey, Konstanz, Germany) (Table III). Each layer was

polymerized separately for 10 seconds followed by an extra-time final polymerization of 60 seconds (Bluephase®, Ivoclar Vivadent, Lichenstein).

Composite	Manufacturer	Composition	Filler	Batch no.
Esthet∙X [®] HD	Dentsply	Bis-GMA adduct	Ba-F-Al-B-Si-glass	
A2	DeTrey,	Bis-EMA adduct	Nanofiller sílica	1006292
Microhybrid	Konstanz, Germany	TEGDMA	(77wt%; 60 vol%)	

Table III: Composite resin; manufacturer, composition, filler and batch no.

Bis-GMA: Bisphenol A dimethacrylate; **Bis-EMA**: Bisphenol A polyethylene glycol diether dimethacrylate; **TEGDMA**: Triethyleneglycol dimethacrylate

Immediately after composite curing, the teeth were kept intact and stored in distilled water at 37°C during 7 days (Heraeus BK 6160, Kelvitron[®] Kp, Wehrheim, Germany).

Cutting method

The specimens were cross-sectioned perpendicularly to the adhesive-tooth interface with a low-speed cutting saw (Accutom 5, Struers, Ballerup, Denmark), under water cooling at 300 rpm, according to the technique described by Sano et al.²⁰, to produce dentincomposite resin sticks with a sectional square area of approximately 1.37mm². After the first cut in x-axis direction, the free residual space between the slices was filled with light-bodied silicone Aquasil Ultra XLV (Dentsply, DeTrey, Konstanz, Germany) (figure 1). Finally, the roots were cut from the crown approximately 2 mm bellow the cementoenamel junction releasing the dentin/composite sticks which were then checked under a optical microscope (M300, Leica, Switzerland) at 40-fold magnification in order to exclude samples with defects. The number of stick specimens obtained per each group was: Group I (Xeno[®] V+) n= 27; Group II (Xeno[®] III) n=24; Group III (OptiBondTM FL) n=41; Group IV (Prime & Bond[®] NT) n=40 and Group V (ClearfilTM SE Bond) n= 37.



Figure 1: Representative images of oclusal and vestibular view of the teeth, before the final root section.

Microtensile bond strength testing

Each stick was bonded to a microtensile sample holder with cyanoacrylate adhesive (Permabond[®] 735, PermabondInternational Co, Englewood, NJ) and then fixed on the microtensile device (Od04-Plus; Odeme Dental Research, Luzerna, Brasil). Specimens were fractured in tensile mode in a universal testing machine (Model AG-I, Shimadzu Corporation, Kyoto, Japan) at a 0.5 mm/min speed and the maximum load (in MPa) at failure was record.



Figure 2: Esquematic diagram from study

After the microtensile testing, the fractured sticks were examined with a optical microscope (M300, Leica, Switzerland) at a 40-fold magnification and the mode of failure was recorded.

Failures modes were classified as: adhesive, if total failure occurred within the adhesive interface; cohesive in dentin (complete failure in dentin); cohesive in composite (complete failure occurred in the composite resin) and, finally, mixed, when simultaneously the adhesive and cohesive failure occurred.

Ultramorphology analysis of dentin substrate by SEM

Two extra dentin disks of 1mm in thickness were obtained by means of two parallel sections of a molar crown (Accutom 5, Struers, Ballerup, Denmark) and then wet-grounded with a sequence of 240-, 400- and 600-grit silicon-carbide sandpaper in circular motion for 60 seconds to obtain a uniform smear layer, fixed in 2.5% glutaraldehyde within a PBS solution for 24 hours and, finally, divided in four samples according the different dentin conditioning preconized for each adhesive system: (1) 36% phosphoric acid; (2) ClearfilTM SE Bond primer; (3) Xeno[®] III primer and (4) Xeno[®] V+. The samples were dehydrated in ascending ethanol series of 50%, 75%, 95% and 100% for at least 2 minutes per step, except the last one during for 4 minutes and immersed in hexamethyldisilazane (HMDS) until complete solvent evaporation.

After chemical dehydration, the specimens were mounted on a specimen aluminium stub using carbon adhesive, sputter-coated with gold-palladium (Polaron E-5000 Sputter-Coater, Polaron Equipment Lta, Watford, U.K.) before SEM analysis with a Hitachi S-4100 microscope (Hitachi, Tokyo, Japan).

Results

Figure 3 and table IV shows the results of the microtensile bond strength of the five adhesive systems tested.

OptiBond[™] FL, Clearfil[™] SE Bond and Prime & Bond[®] NT had the best performance in microtensile bond strength test. "Spontaneous" interfacial debonding occurred in 11 cases of the Xeno[®] V+ group, which presented inferior mean values. Additional similar pre-test failures were only found in two samples of Xeno[®] III.



Figure 3: Box plot graphic for microtensile bond strength values distribution within groups

Table IV: Descriptive statistics for microtensile bond strength values of groups. Mean, standard deviation (SD), minimum and maximum values in MPa. Same upper case letters are not satistically different.

Group	Adhesive Systems	n	Mean ±SD	Min	Max	95% CI
I	Xeno [®] V+	27	3.70±5.01 ^A	0.00	21.48	[1.72, 5.68]
II	Xeno [®] III	24	18.94±13.87 ^B	0.00	42.55	[13.08,24.80]
	OptiBond [™] FL	39	43.29±12.74 [°]	20.54	69.87	[39.16,47.42]
IV	Prime & Bond [®] NT	40	39.64±15.06 ^C	13.35	67.44	[34.83,44.46]
V	Clearfil [™] SE Bond	37	42.80±10.65 [°]	18.36	66.84	[39.24,46.35]

Mean adhesion values for the five groups were compared using one-way ANOVA setting the significance level at α =0.05 and considering zero as the value for pre-test failures. Post-hoc analysis was performed with Tukey HSD multiple comparisons test. There were no real outliers and the data was normally distributed for all groups (p>0.05) except Xeno[®] V+ (p=0.001), as assessed by box plot and Kolmogorov-Smirnov test. There was no homogeneity of variances, as assessed by Levene's Test of Homogeneity and Variance (p<0.05). Microtensile bond strength values were statistically significantly different between groups of adhesives F(4,162)=62.50, p<0.01, ω^2 =158.99. Bond strength values increased from the Xeno[®] V+ group (3.70±5.01 MPa), to Xeno[®] III (18.94±13.87 MPa), to Prime & Bond[®] NT (39.64±15.06 MPa), to ClearfilTM SE Bond (42.80±10.65 MPa) and to OptiBondTM FL (43.29±12.74 MPa), in that order.

Post-hoc analysis revealed that the increase from Xeno[®] V+ to Xeno[®] III (15.24, 95% CI [5.78,24.69]), from Xeno[®] V+ to Prime & Bond[®] NT (35.94, 95% CI [27.55,44.34]), from Xeno[®] V+ to ClearfilTM SE Bond (39.10, 95% CI [30.57,47.63]) and from Xeno[®] V+ to OptiBondTM FL (39.59, 95% CI [31.16,48.03]) was statistically significant (p<0,01). As shown in Table V increases in mean bond strength values from Xeno[®] III to Prime & Bond[®] NT, ClearfilTM SE Bond and OptiBondTM FL groups were also statistically significant.

There was a statistically significant difference between means (p<0.05), thus we can reject the null hypothesis.

	(J)	Mean Difference (I-J)	Std. Error	р	95% Confidence Interval	
(I) Group						Upper
					Lower Bound	Bound
Xeno [®] V+	Xeno [®] III	-15.24	3,43	,000	-24,69	-5,78
	Optibond [™] FL	-39.59 [*]	3,06	,000	-48,03	-31,16
	PB [®] NT	-35.94	3,04	,000	-44,34	-27,55
	Clearfill [™] SE Bond	-39.10 [*]	3,09	,000	-47,63	-30,57
Xeno [®] III	Xeno [®] V+	15.24 [*]	3,43	,000	5,78	24,69
	Optibond [™] FL	-24.36*	3,17	,000	-33,10	-15,61
	PB [®] NT	-20.70*	3,15	,000	-29,41	-12,00
	Clearfill [™] SE Bond	-23.86*	3,20	,000	-32,69	-15,02

Table V: Multiple comparisons for groups I and II (Tukey HSD test). Mean difference of microtensile bond strength values between groups in MPa

The crosstabulation, observed and expected frequencies for each cell of the design are found in the Failure*Group Crosstabulation table (Table VI), as shown below:

Failure * Group Crosstabulation								
				Group				
			Xeno [®] V+	Xeno [®] III	Optibond [™] FL	$PB^{\mathbb{R}} NT$	Clearfill [™] SE Bond	Total
Failure	Ad	Count	16 ^a	13 ^b	0 _c	4 _c	2 _c	35
		% within Failure	45,7%	37,1%	0,0%	11,4%	5,7%	100,0%
	DC	Count	0 _a	3 _a	2 _a	0 _a	4 _a	9
		% within Failure	0,0%	33,3%	22,2%	0,0%	44,4%	100,0%
	CC	Count	0 _a	1 a	31 _b	22 _b	25 _b	79
		% within Failure	0,0%	1,3%	39,2%	27,8%	31,6%	100,0%
	Mix	Count	0 _a	5 _a	6 _a	14 _a	6 _a	31
		% within Failure	0,0%	16,1%	19,4%	45,2%	19,4%	100,0%
Total		Count	16	22	39	40	37	154
		% within Failure	10,4%	14,3%	25,3%	26,0%	24,0%	100,0%

 Table VI Failures mode percentage of the debonded specimens for each group: Ad - Adhesive failure DC - Dentin cohesive failure; CC - Composite cohesive failure; Mix - Mixed failure;

Each subscript letter denotes a subset of Group categories whose column proportions do not differ significantly from each other at the .05 level.

Chi-square test for association was conducted between failure type and adhesive system. There was a statistically significant association between failure type and adhesive system, X^2 (12)= 112.64, p<0.05

There was a moderately strong association between failure type and adhesive system, V= 0.49, p<0.01. Adhesive failures were associated with both Xeno[®] V+ and Xeno[®] III. Cohesive composite fractures were associated with both OptiBondTM FL, Prime & Bond[®] NT and ClearfilTM SE Bond.



Figure 4: Representative images of the different failure modes: **Ad** - Adhesive failure; **CC** - Composite cohesive failure; **DC** - Dentin cohesive failure; **Mix** - Mixed failure.

SEM observations

Figure 5 is a SEM representative image of the smear layer adhered to dentin surface and partially occluding the dentinal tubules before different adhesive dentin conditionings.



Figure 5: SEM representative image(6000x) illustrating the smear layer covered dentin.

Concerning the ultra morphology analysis of the adhesive conditioned dentin, the SEM analysis showed different patterns (Figure 6).



Figure 6: Representative SEM images (6000X) of dentin treated with: (A)- 36% phosphoric acid for 15 seconds and rinse with water; (B)- Clearfil[™] SE Bond primer; (C)- Xeno[®] III; (D)- Xeno[®] V+.

The analysis of the dentin disks under SEM showed that after etching with 36% phosphoric acid smear layer was completely removed and subjacent dentin and dentinal tubule orifices were visible and their input was expanded.

The primer of two-step self-etching adhesive system, Clearfil[™] SE Bond, removed most smear plugs and showing the underlying dentinal tubules and also a partially visible, dissolved smear layer in the intertubular area.

Unlike to phosphoric acid and Clearfil[™] SE Bond primer, the patterns of dentin surface created by one-step self-etch adhesive systems Xeno[®] III and Xeno[®] V+ showed that smear plugs were not removed, or only partially, and a partially dissolved smear layer was visible in the intertubular area.

Discussion

Today the current challenge in adhesive dentistry is to ensure the long-term success, making the adhesive-tooth interfaces more resistant against aging². One of the most important issues of recent adhesive materials is its durability²¹, which seems to be dependent either on the adhesive's formulation and the bonding strategy²¹.

The transition between the restorative material and the dental hard tissue must be continuous to increase the survival probability of the restoration²². In spite of adhesive bond strengths to enamel are predictable, satisfactory and stable when etch-and-rinses systems are employed^{23, 24} bonding to dentin is a much more complex issue, due to the nature of this substrate²⁴, namely its higher organic content and the presence of fluid and odontoblastic processes in the tubules²³. The long-term durability appears to be influenced by substrate and polymer stability, activity of metal matrix proteins (MMPs) and the ongoing decalcification by bacterial generated acids²⁵.

No internationally standardization test protocols yet exists for the testing adhesives systems²⁶. Therefore, variable methods and parameters have been employed by the different laboratories making difficult the comparison across studies²⁷.

The interface between restoration and tooth is exposed to different challenges in oral cavity such as forces that act in different directions and simultaneously² or thermal oscillations that can induce cumulative stresses and progressive interface degradation⁹. By definition, the ideal bond strength test should be easy to perform, low technique-sensitivity, relatively fast, unsophisticated and inexpensive⁷, and, most important, capable to simulate biomechanics conditions of restored teeth. Bond strength testing is the method most used for the assessment of bonding effectiveness to enamel and dentin^{28, 29} including different mechanical methods³⁰. These tests are used to evaluate the ability of a restorative material or dentin bonding system to establish a bond to a biological substrate²².

Generally, bond strength can be measured by macro and micro test set-ups, basically depending upon the bonded size area⁷. The bond strength tests results can be affected by several parameters, like, operator, research group/institute, adhesive system, adhesive class, substrate preparation, substrate origin and composites flexural modulus³¹. The characteristic of the bonding substrate plays a major role on the quality of adhesion⁶. Clinically relevant substrates include caries-affected, caries infected, sclerotic, deep and bur cut dentin³². In the present study bond strengths were measured under a sound dentin substrate that always play a important role in surrounding walls of cavities design. Besides the same composite resin was used combined with each adhesive system studied for cutting off the possible influence of resin composite modulus development.

The shear bond-strength test is the most commonly used³⁰, namely between manufacturers, because it is easy and fast to perform⁷. However, some problems have been related to the shear bond strength test, as unrealistic stresses are produced within the reaction zone³¹. Microtensile bond strength test allows measurements of the tensile bond strength on very small surfaces, about 1 mm^{2, 20, 33}. This method allows multiple specimens to be prepared from each tooth³⁴, measuring bond strength at critical areas³¹, with a more uniform stress distribution in the reaction zone and a higher reliable correlation with clinical retention loss³¹.

There are several critical factors that influence the results of the microtensile bond strength test, such as diameter of the stick, type of jig, trimming³⁵ and storage of bonded specimens in water³¹.

In this test, the loading force passes through the tooth substrate and composite resin before the adhesive interface³⁶. Thus, the subsequent stress concentration could explain the frequent cohesive failure in the tooth substrate³⁶, which not reflect the true bond strength²⁶.

Microtensile bond strength tests have a number of advantages, such as: more adhesive failures and fewer cohesive failures^{27, 29}; measurement of higher interfacial bond strengths^{27,29}; allows testing on very small surfaces^{27,29, 37} or in irregular surfaces^{27,29}; means and variances can be calculated for single teeth^{27, 29}; and facilities examination of failed bonds by scanning electron microscopy^{29,27}. However, some disadvantages were also described for the microtensile bond strength test, as the labour intensity, technical demand and dehydration potential of these smaller samples²⁷.

In the present study, the best performing adhesive systems was the 3-step etch-andrinse OptiBondTM FL (43.29±12.74), followed by 2-step self-etch Clearfil SETM Bond (42.80±10.65) and Prime & Bond[®] NT (39.64±15.06) without no statistical differences found between them. OptiBondTM FL has already showed very favourable laboratory^{38, 39} and clinical performance^{28, 40, 41} Pashley *et al*⁴ referred that 3-steps etch-and-rinse adhesives are more durable than 2-step etch-and-rinse adhesives, due to the first one has the advantage and opportunity to use each step for essential multipurpose objectives.

OptiBond[™] FL bonding resin composition has cross-linking monomers. The relative amounts of Bis-GMA, TEGDMA and UDMA presents is this adhesive system may have a meaningful influence on the viscosity of the uncured adhesive resin and on the mechanical properties of the cured resin⁴². TEGDMA has high flexibility which is compensated by the rigidity of Bis-GMA⁴². Some studies that used OptiBond[™] FL presented very scatter bond strength values. Phrukkanon *et al*⁴³ (1998) obtained 20.2±5.0 MPa which is lower comparing

with the present study. Conversely, Heintze & Zimmerli²⁶ (2011) in a study about the relevance of in vitro tests of different adhesive systems, registered 48.0 ± 13.7 MPa to OptiBondTM FL, which is similar to those obtained in the present work. Along with two-step self-etch adhesives, three-step etch and rinse adhesives are considered the *gold standards* for dentin adhesion.

Presenting also good performance, Prime & Bond[®] NT, contains an acidic phosphonated monomer (PENTA) which can interact with calcium ions left on dentin surface²¹. This adhesive system is filled with nanoparticles that may help to establish a thicker and more uniform resin film thickness that stabilizes the hybrid layer⁴⁴. Prime&Bond[®] NT had a mean microtensile bond strength of 39.64MPa. The performance of this adhesive has been evaluated by other authors which registered lowers values than de present study^{37,45}.

Clearfil SE[™] Bond, though belonging to the group of "mild" self-etch adhesives⁹, also had a high performance concerning bond strengths. This adhesive system was the only self-etch obtaining microtensile bond strength values comparable to those etch-and-rinse adhesives and no statistical differences were found between them.

Osorio *et al.*²¹ (2008) stated that high percentage of camphorquinone in this adhesive might improve the degree of polymerization and the presence of 10-methacryloxydecyl dihydrogen phosphate (10-MDP) which can contribute to the higher bond stability due to its chemical adhesion with tooth tissues⁴². In fact, this 10-MDP molecule can chemically bond to calcium of hidroxiapatite, according to the adhesion decalcification concept, forming a stable calcium-phosphate salt, along with only a limited surface-decalcification effect. 'Mild' self-etch adhesives indeed only superficially interact with dentin, and hardly dissolve hidroxiapatite crystals, but rather keep them in place, forming a thin submicron hybrid layer³. In this study, microtensile bond strength results for ClearfilTM SE Bond were 42.80±10.65 MPa. In the literature, similar results were found to this adhesive system by other authors^{15,26}.

Clinicians prefer materials with an easy, simplified application. However, these simplified adhesives can be associated to a less optimal clinical effectiveness⁹.

In this present study the adhesive system with lowest performance was the Xeno[®] V+ (DentisplyDeTrey, Konstanz, Germany), followed by the Xeno[®] III (DentisplyDeTrey, Konstanz, Germany). Xeno[®] V+ presented a mean of 3.70±5.01 (MPa) and 11 pre-test failures within 27 specimens in total. Another study, by Nikhil *et al.*⁴⁶ (2011), also demonstrated a lower performance for Xeno[®] V+ and referred that the adhesive system bond strength can be associated to absence and presence of HEMA, which is absent in case of Xeno[®] V+ (HEMA-free). In adequate concentration, this monomer can contribute for bond strength due to its hydrophilic nature that makes it an excellent adhesion-promoting monomer and by enhancing wetting of dentin. Nevertheless, HEMA-free one-step adhesives

are complex blends of hydrophilic/hydrophobic ingredients, water and solvents, prone to phase separation, which can account partially for their lower bonding effectiveness⁴⁷. On the other hand, Xeno[®] V+ adhesive system contains tertiary butanol, which is related to a more stable formulation than those containing ethanol, according El-kholany *et al*⁴⁸. Although a long shelf-life has been attributed for this adhesive by the manufacturer, possible alterations in Xeno[®] V+ components can also explain the lowest results reported in this study.

In this study Xeno[®] III also presented, comparatively, lower bond strength values. In high amounts, HEMA, which is a Xeno[®] III component, may have deteriorating effects on the mechanical properties of the resulting polymer⁴². For this adhesive system, Loguercio *et al.*⁴⁹ reported a higher bond strength result, 28.3MPa, while Bortolloto *et al.*⁵⁰ registered a mean of 23.8 MPa, and Amaral *et al.*⁵¹ showed a mean of 19.9MPa in microtensile bond strength for this one-step self-etch adhesive.

Simplified one-step self-etch adhesive system does not provide the formation of a high quality hybrid layer compared to 2-step self-etching primers and conventional etch & rinse adhesives¹⁵. One-step self-etch adhesives composition are a complex mixture of hydrophobic acid monomer, hydrophilic resins, solvent and water^{15,29,52}. The lack of hydrophobic resins for hybrid layer formation¹⁵ and, consequently due to their hydrophilic nature, these adhesives systems may act as permeable membranes and absorb significant amounts of water, even when polymerized⁵² which can compromise bond strength to dentin and influence the failure mode¹⁵. Moreover, monomer degradation has several adverse effects on the performance of dental adhesives, predominantly by the deterioration of bond strength and inducing morphological changes at the adhesive/dentin interface⁵³.

In the presented study, the mode of failure was related with the adhesive system. The adhesive failure was associated to low bond strengths values, meaning for the Xeno[®] V+ and Xeno[®] III. On the other hand, the higher bond strength values were correlated with cohesive failures that occurred in the best performance adhesive systems OptiBond[™] FL, Clearfil[™] SE Bond and Prime &Bond[®] NT.

Similar results were reported in other study. Ceballos *et al.*⁴⁴ (2003) correlated the bond strength values with mode of failure. Low bond strengths were associated with adhesive failures, while cohesive fractures were seen at higher bond strengths.

Scherrer *et al.*⁵⁴ (2010) stated that the common cohesive failures that occurred in microtensile bond strength tests may be due to the errors in the alignment of the specimen along the long axis of the testing device or to the introduction of microcracks during cutting. In the present study, cohesive failures occurred frequently, but correlated significantly well with greater adhesion values. Concerning this point, it can be understood that, at least, the adhesive bonding to dentin was stronger than the registered value and therefore of the cohesive strength of resin or dentin.

Statistical analysis showed 11 pre-test failures within Group I (Xeno[®] V+) and 2 for Group II (Xeno[®] III). The high number of the pre-test failures represented an additional point for the scatter in microtensile bond strength results⁵⁴. These values can be treated by different manner by researchers^{31,54}. In the present study they were considered as zero in the statistical analysis, which explain the decrease in mean values and the increase in standard deviation, but reflects truly the concern about the weakness of the produced adhesive interface⁵⁵.

Concerning the future research perspectives, it will be valuable improving the standardization of test conditions, studying the same adhesives with different methodologies and even with different operators, as well as conducting *in vitro* tests after aging, complemented with clinical trials. Furthermore, researches evaluating other bonding properties and different adhesive bonding approaches should be targeted.

Conclusions

Within the limitations of this in vitro study, it can be concluded that:

- Etch-and-rinse adhesives and two-step self-etch adhesives showed higher microtensile bond strength values than one-step self-etch adhesives.
- Adhesive failure mode was correlated to lower bond strength results, while the cohesive failures are more common with higher adhesion values.

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